A Modified Transparent Angiography Catheter: Preliminary In Vivo and In Vitro Evaluations

Hyo S. Ahn and James H. Anderson

Most of the serious neurologic complications related to angiography are embolic in nature. Meticulous catheter flushing techniques have been suggested to reduce embolic complications [1]. An experimental catheter with a 20-cm-long transparent proximal section has been evaluated to determine its usefulness in monitoring catheter flushing procedures and inadvertent injections of emboli. Catheters that are transparent throughout their entire length may not have enough radiopacity or torque control to enable adequate manipulation. Replacing the proximal portion of the catheter with a transparent tubing preserves maneuverability of the original catheter while allowing direct visualization of the extravascular portion of the catheter lumen. We report our initial experience with this modified transparent catheter.

Materials and Methods

Catheter Design

The modified catheter was constructed by replacing the proximal 20-cm portion of a 5-French polyethylene cerebral angiography catheter* with a transparent polyethylene tubing (ID, 1.40 mm; OD, 1.90 mm).† One end of the tubing was bonded to the original catheter with cyanoacrylate glue, and the other end was connected to a blunt-tip needle (16 g) (Fig. 1).

In Vitro Evaluation

In vitro experiments were carried out to evaluate the use of the catheter in detecting inadvertent introduction of emboli. Small Gelfoam particles (3 x 3 x 3 mm), suspended in saline, were loaded into 3- and 10-ml plastic syringes and injected slowly (approximately 1 ml/sec) through the modified transparent catheter. When a Gelfoam particle was detected traveling through the transparent portion of the catheter, the injection procedure was immediately terminated and the particle was retrieved into the syringe by withdrawing the plunger. This experiment was repeated 20 times with each syringe.

* Becton Dickinson, Rutherford, NJ.
† Clay Adams, Parsippany, NJ.
‡ Travenol Laboratories, Inc., Deerfield, IL.

Received April 27, 1988; accepted after revision October 25, 1988.

Both authors: The Russell H. Morgan Department of Radiology and Radiological Sciences, Johns Hopkins Medical Institutions, 601 N. Wolfe St., Baltimore, MD 21205. Address reprint requests to H. S. Ahn.

Results

Gelfoam particles injected into the catheter were easily detected as they passed through the transparent portion of the catheter. All 40 particles were easily retrieved before they could exit from the catheter tip.

Transparency of the catheter allowed us to evaluate the effectiveness of various flow rates in clearing blood in the lumen under direct visual inspection. When the blood-filled catheter was connected to a volumetric infusion pump with infusion rates between 10 and 100 ml/hr, clearing of blood in the transparent portion of the catheter was slow. Layering of blood in the dependent portion of the catheter persisted throughout the experiment (3 min). Complete clearing of blood in the transparent portion of the catheter was achieved within 30 and 90 sec with a flow rate of 500 and 250 ml/hr, respectively. Once complete clearing of the transparent portion of the catheter was achieved, a decrease in the infusion rate to 30 and 50 ml/hr effectively prevented reflux of blood into the transparent portion of the catheter.

Discussion

The frequency of all neurologic complications of cerebral angiography varies from 0.9% to 4.6% [2–4]. Most complications related to catheter angiography are caused by emboli [1]. The reported frequency of inadvertent embolization during cerebral angiography is 0.4% by Olivecrona [4] and 0.9% by Pettersson et al. [5]. Emboli originate from three main sources: (1) dislodged thrombus or plaque from the intima of vessels during manipulation of catheters or guidewires, (2) thrombus dislodged from the inner surface of the catheter during injections of contrast material or saline, or by guidewire manipulation, and (3) inadvertent injections of blood clots and foreign bodies such as air bubbles and cotton fibers. Damage to vessel walls is minimized by using small-diameter catheters made of soft plastic [6]. Various technical improvements have been reported to reduce embolic complications. Heparin-coated catheters reduce thrombus formation in the inner surface of the catheters [7]. Closed systems of contrast media and flush solutions have been advocated to avoid contamination by foreign bodies [8–10]. Cronqvist et al. [11] suggested that a constant infusion of saline instead of intermittent injections may be of value in preventing intraluminal clot formation. Kido et al. [7] indicated that the rate of thrombus formation on the inner surface of the catheter is largely related to the amount of blood that is allowed to reflux into the catheter lumen. An ideal infusion rate for a particular patient is difficult to determine and may vary according to the patient’s blood pressure and size of the catheter being used. To avoid overhydrating the patient, a low infusion rate that can effectively clear the catheter of blood is desirable. However, as we observed, flushing the catheter with a low infusion rate resulted in layering of blood in the dependent portion of the catheter. Therefore, it is suggested that the catheter be flushed at a high infusion rate for a few seconds at the beginning of the flush and then decreased to an effective low rate. The modified catheter may not have advantages over regular catheters in preventing injection of thrombi formed in the nontransparent portion of the catheter but it may decrease the occurrence of thrombi formation on the inner surface of the catheter, since one can directly visualize and improve the status of flush in the catheter. Our results indicate the modified transparent catheter may be of value in preventing the inadvertent injections of emboli and in maintaining thorough flushing of the catheter.

In daily clinical practice, some 20–30 cm of the catheter would remain extravascular. By replacing some of this extra­vascular portion of the catheter with transparent material, an extra margin of safety can be achieved while maintaining the original properties of radiopacity and stiffness. Since the transparent tubing does not have a sufficient stiffness for torque control, the length of the transparent portion is adjusted to provide a sufficient portion of the original catheter proximal to the skin for catheter manipulation. In the present study, a 5-French catheter was used to make the modified transparent catheter. However, this modification can be easily achieved on any size catheter. Injector-connecting tubes and IV-infusion tubings now being used in angiographic proce­dures are transparent as a safety feature to reduce the possibility of inadvertently injecting air bubbles, emboli, and so forth. Angiographers would benefit by having extended transparent tubings as provided by the modified catheter. This prototype catheter was assembled purely for evaluation purposes. We do not recommend gluing the catheters together for clinical use. The bonding site remained intact through the experiments but we did not measure the force required to break the bond.

The clinical efficacy of a modified transparent catheter needs to be evaluated through clinical trials. The results of the preliminary work are encouraging and should stimulate manufacturers to consider providing such a catheter for evaluation and possible clinical use.

REFERENCES