Study of the Patency of Small Arterial Branches after Stent Placement with an Experimental in Vivo Model

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BACKGROUND AND PURPOSE: The patency of intracranial perforating arteries after stent placement is unknown despite the general clinical use of intracranial arterial stenting.

METHODS: We deployed stainless steel stents in the abdominal aorta across the lumbar artery in eight normal rabbits in which the diameters of the abdominal arterial vessels were similar to those of human intracranial arteries. We evaluated the patency via angiographic and scanning electron microscopic methods 3 months after stent placement. Histopathologic evaluation was also performed for one rabbit.

RESULTS: The lumbar arteries were patent, even when stent struts crossed the ostium, except in one rabbit in which intimal dissection occurred intraoperatively. The scanning electron microscopy showed that the regenerative endothelium had grown onto the strut at the ostium of the lumbar artery.

CONCLUSION: We confirmed the patency of the lumbar arteries in this study by using normal rabbits. Thus, intracranial stenting may not pose a risk of occluding perforating arteries of the same diameter of the lumbar artery, even if stent struts cover the ostium.

One major concern related to intracranial stenting is whether perforating arteries will become occluded after stent placement. The relationship between the abdominal aorta and the lumbar arteries in the rabbit is anatomically similar to that between the major intracranial arteries and the perforating arteries in humans with regard to diameter and angle of origin. In this study, we performed stent placement in the abdominal aorta across the ostium of the lumbar artery in normal rabbits and evaluated the status of the ostium 3 months after stent placement by angiographic, scanning electron microscopic, and histopathologic methods.
coating with 20 nm of gold, we examined the patency and the degree of re-endothelialization at the ostia of the lumbar arteries.

**Histopathologic Evaluation**

One rabbit’s stented aorta was evaluated for the neointimal composition at the ostium of the lumbar artery by using immunohistopathologic methods (case 8). After exsanguination, the stented artery was harvested and then fixed with 10% neutral buffered formalin. The stented artery was carefully cut with a tungsten knife in 4–5-μm-thick sections. The cut sections were stained with hematoxylin and eosin to examine cell composition. The other sections were examined by immunohistochemical staining to identify the specific cell types with antibodies for endothelial cells (factor VIII) and smooth muscle cells (alpha-actin).

<table>
<thead>
<tr>
<th>Rabbit</th>
<th>Diameter of Aorta (mm)</th>
<th>Diameter of Lumbar Artery (μm)</th>
<th>Deployed Stent Diameter (mm)</th>
<th>Stent-to-Artery Ratio</th>
<th>Angiographic Complication</th>
<th>Patency of Lumbar Artery</th>
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* In this case, the stent was delivered without a guidewire and caused intimal dissection.
† This rabbit became paraparetic after stenting, although the lumbar artery was patent on the post-stenting angiogram.
‡ Follow-up angiography of the rabbit was performed 1 week after stenting.

Results

**Angiographic Findings**

The angiographic results are summarized in the Table. The diameter of the aorta was measured with a measure wire. The deployed stent diameter was based on the manufacturer’s information. The diameters of lumbar arteries were measured by using the scale measure on the scanning electron microscopic images. They ranged from 473 to 802 μm (average diameter, 643 μm). The diameter of the lumbar artery for cases 3 and 8 were not measured because no stent struts crossed the ostia of the stented aorta. These endothelial cells appeared to have been growing onto the struts crossing the ostium of the lumbar artery, although the covering was incomplete at this time point (Fig 3). The extension of regenerated endothelial cells encroaching on the ostia of lumbar arteries was also observed in several cases (Fig 3A), but the degree of narrowing due to this extension was not significant at this point. The diameters of lumbar arteries, measured by using a scale measure on the scanning electron microscopic image, ranged from 473 to 802 μm (average diameter, 643 μm) (Table). The smaller branches could not be evaluated because no stent struts crossed the ostia of these branches.

The pathomorphologic evaluation of the ostium of the lumbar artery and the status of the re-endothelialization were investigated by scanning electron microscopy after follow-up angiography. The scanning electron microscopic findings for the rabbit that had become paraparetic after stenting (case 5) revealed that the lumbar artery in the stent was patent without thrombus. The diameter of the lumbar artery was 729 μm, as measured by using a scale measure on the scanning electron microscopic image. The endothelial integrity was injured along the struts by stent expansion (Fig 2). The underlying smooth muscle fiber was also exposed in that part of the luminal surface, but we suspected that this damage was caused during postprocessing because the same observation was made with scanning electron microscopy performed at 3 months after stenting.

In all other rabbits, scanning electron microscopy performed 3 months after implantation showed the patency of lumbar arteries and regenerated endothelial cells covering the stent struts in contact with the aorta. These endothelial cells appeared to have been growing onto the struts crossing the ostium of the lumbar artery, although the covering was incomplete at this time point (Fig 3). The extension of regenerated endothelial cells encroaching on the ostia of lumbar arteries was also observed in several cases (Fig 3A), but the degree of narrowing due to this extension was not significant at this point.

fore suspected that distal embolization might have caused a spinal cord infarction. Follow-up angiography performed 3 months after implantation in six rabbits showed the patency of the lumbar arteries without significant luminal narrowing (Fig 1).
Histopathologic Findings

Macroscopic analysis of the stented arteries revealed that the stent struts that were in contact with the aortic wall were covered by a thin membranous layer, and the ostia of the lumbar arteries were widely open, regardless of whether a stent strut crossed the lumbar artery. Microscopic analysis of sections stained with hematoxylin and eosin revealed stretching of the media of the aorta by the strut and reactive smooth muscle cell proliferation around the strut. This cellular component was confirmed to be smooth muscle cells by immunohistochemical staining for alpha-actin. The luminal surface of the stented artery was lined with a monolayer of cells resembling regenerative endothelial cells, although immunohistochemical staining for factor VIII failed to show any immunoreactivity. Cells resembling regenerative endothelium were also found on the strut across the ostium (Fig 4).

Discussion

Several cases of successful intracranial stenting have recently been reported with the advent of flexible coronary stents (1–9). According to these reports, intracranial stenting may be safe and useful for the treatment of wide-necked aneurysms and for elastic recoil or dissection after percutaneous transluminal angioplasty for atherosclerotic lesions. However, stenting of intracranial atherosclerotic lesions has not yet been widely adopted, partially because of many unresolved questions. One concern is whether stent placement may lead to occlusion of perforating arteries originating from the stented vessel, although no cases of symptomatic occlusions of perforating arteries after intracranial stenting have been reported in the clinical literature (2).

In experimental work, several studies have investigated the patency of side branches from the stented arteries after stent placement. Wakhloo et al (10) reported that the cervical branches originating from the canine vertebral arteries within the stented segments remained angiographically patent 9 months after self-expanding nitinol stent placement. Whitbread et al (11) assessed the patency of the renal artery 6 months after placing a Wallstent across the orifice of the renal artery in six pigs. In their study, no renal arteries were occluded based on follow-up aortograms, and scanning electron microscopy of the stented aorta showed partial endothelialization of the stent but the renal artery origins remained widely patent.

Fig 1. Representative case (case 4).
A, Diameter of abdominal aorta is measured by using a measure wire.
B, Angiography is performed before stenting.
C, Just after stenting, angiography is performed to evaluate the patency of the lumbar artery (arrow).
D, Follow-up angiogram, obtained 3 months after stenting, confirms that the lumbar artery remains patent (arrow).

Fig 2. Case 5. Scanning electron microscopic findings obtained 1 week after stenting for the rabbit that became paraparetic after stenting reveal that the lumbar artery (asterisk) in the stent is patent without thrombus. The diameter of the lumbar artery is 729 μm. Endothelial integrity is injured along the struts by stent expansion (arrows), and underlying smooth muscle fiber is exposed in part of the luminal surface because of post-processing (original magnification ×100).
patent. Malina et al (12) also showed that the renal arteries remained patent without any significant decrease in the renal blood flow and renal dysfunction after placing Gianturco and Palmaz stents. Birch et al (13) compared the effects of crossing renal artery ostia with three various stents (Wallstent, Palmaz, and Memotherm). In all cases that used the Wallstent (nine cases), all ostia were patent despite that the most organized collagen matrix on the strut was in contact with the aorta. However, in one of nine cases that used the Palmaz stent and in 12 of 13 cases that used the Memotherm stent, the neointima caused partial ostial occlusion. The authors suggested that the tissue reaction to the stent was dependent on the shape and composition of the struts and that the fine rounded stainless steel struts excited less reaction.

We studied the patency of lumbar arteries after stenting using normal rabbits to investigate whether perforating arteries, smaller than the renal artery in diameter, would be occluded after intracranial stenting. ACS/GUIDANT RX Multi-link stents, made of a laser-cut stainless steel, were used in this study. The characteristics of this stent include good conformability due to the very thin flat strut and the composition of the strut. Rabbits were used in this study because the relationship between major intracranial arteries and perforating arteries originating from these arteries in humans approximated that of the abdominal aorta and lumbar arteries in the rabbit with respect to diameter and angle of origin. In previous reports regarding microsurgical anatomy, the diameters of the middle cerebral, vertebral, and basilar arteries ranged from 2.4 to 4.6 mm (average, 3.9 mm), from 2.0 to 5.7 mm (average, 3.5 mm), and from 3.0 to 5.5 mm (average, 3.9 mm), respectively (14, 15). The diameter of the perforating arteries ranged from 100 to 600 μm in the vertebral artery, from 200 to 500 μm in the basilar artery, and from 120 to 1250 μm in the middle cerebral artery. In our series, the average diameter of abdominal aorta and lumbar artery originating from the abdominal aorta were 2.9 mm and 643 μm, respectively.

Our results showed the patency of lumbar arteries without significant luminal narrowing and flow reduction on the follow-up angiograms of all rabbits. This was confirmed by scanning electron microscopy performed 3 months after stenting, which showed that the regenerative endothelium had grown along the struts crossing the ostium of lumbar artery. However, there were still bare portions of the struts crossing the ostium. Endothelialization in these portions might lag behind the portion in contact with the luminal wall in cases of complete re-endothelialization because of blood flow. It is unclear which kind of cellular response may happen in this bare portion over a longer period, although there are several likely possibilities. These bare portions may remain “bare.” Endothelial cells may completely encompass the stent struts without ostial occlusion. Proliferative smooth muscle cells and regenerative endothelium may cover the ostium completely. The fate of the bare portion will be determined by the degree of the ostial coverage by the stent struts.

Regarding tissue response after stent placement, Schatz et al (16, 17) suggested that stents were covered initially by a thin layer of thrombus and fibrin that was later replaced by neointimal muscular proliferation and that thrombosis was essential for healing but must be controlled. Grewe et al (18) also reported the same tissue response. Schatz (17) sug-
gested that the successful vascular stent should depend on minimal thrombosis and rapid endothelialization and that stent-induced thrombus formation could be avoided successfully with anticoagulant and antiplatelet agents. The shape and composition of the stent strut might be important factors for ostial occlusion. Antiplatelet therapy after stent placement might also play an important role in preventing ostial occlusion. We performed antiplatelet therapy consistent with previous reports for 1 month after stenting for this study (19, 20), but we might need to continue longer term antiplatelet therapy to lead to complete endothelialization around struts crossing the ostium with minimal muscular proliferation. This longer term antiplatelet therapy also might be necessary to prevent the extension of regenerative endothelial cells encroaching on the ostia of lumbar arteries, although significant narrowing and restriction of the ostia were not observed 3 months after stenting.

**Conclusion**

We confirmed patency of the lumbar arteries branching from the stented abdominal aorta 3 months after stent placement in normal rabbits. These results suggest that intracranial perforating arteries, 643 μm in average diameter, might also remain patent for the first 3 months after implantation. However, a longer term study of more than 3 months, with atherosclerotic models, is required to extend these results.

**References**