Impaired Default Mode Network on Resting-State fMRI in Children with Medically Refractory Epilepsy

E. Widjaja, M. Zamyadi, C. Raybaud, O.C. Snead, and M.L. Smith

ABSTRACT

BACKGROUND AND PURPOSE: Resting-state networks including the DMN have been shown to be abnormal in adults with temporal lobe epilepsy. However, little is known about the DMN in children with medically refractory epilepsy. The aim was to determine whether there was a difference in the DMN in children with medically refractory epilepsy relative to controls.

MATERIALS AND METHODS: Eleven children with medically refractory epilepsy and 11 age-matched healthy controls underwent resting-state fMRI. IC analysis was used to identify the DMN. A random-effects analysis was performed on the Z-maps of the DMN within each group and between groups. We calculated the temporal correlation coefficients of pairs of ROIs: PCC/PCUN, mPFC, and left and right lateral parietal cortices. The relations between z scores of temporal correlation coefficients of pairs of ROIs and clinical seizure parameters and IQ were assessed.

RESULTS: The patients demonstrated decreased DMN connectivity in the PCC/PCUN, bilateral lateral parietal cortex, and anterior and midcingulate relative to controls. There was reduced connectivity between the mPFC–right lateral parietal cortex, the PCC/PCUN–left lateral parietal cortex, and the PCC/PCUN–right lateral parietal cortex pairs of ROIs in patients compared with controls. There were no significant correlations between the z scores of temporal correlation coefficients of the 6 pairs of ROIs in patients and age of seizure onset, duration of epilepsy, number of medications, seizure frequency, and IQ.

CONCLUSIONS: We have found reduced connectivity in the DMN in children with medically refractory epilepsy. Further studies are needed to determine whether different seizure types have different effects on the DMN and whether the impaired connectivity is related to cognitive functions subserved by the DMN.

ABBREVIATIONS: DMN = default mode network; EEG = electroencephalogram; IC = independent component; IQ = intelligence quotient; mPFC = medial prefrontal cortex; PCC/PCUN = posterior cingulate cortex/precuneus

Functional connectivity is defined as the temporal synchronization of low-frequency fluctuations (0.01–0.1 Hz) arising from spontaneous neuronal activities in distant brain regions.1 The spontaneous fluctuations are measured at rest, the method is referred to as “resting-state” fMRI, and the identified brain networks are referred to as resting-state networks. The DMN, which is one of the resting-state networks, is a prominent large-scale brain network that includes the PCC/PCUN, mPFC, lateral parietal cortex, and medial temporal lobes. The DMN has high resting metabolism, deactivates during cognitively demanding tasks,2 and demonstrates increased activity during high-level social cognitive tasks.3 Individual brain regions that make up the DMN are involved in the integration of autobiographic memory, self-reflective processes, and social cognitive functions.4 The PCC/PCUN is activated during tasks that involve autobiographic memory and self-referential processes.5 The mPFC is associated with social cognitive processes related to self and others.6 The medial temporal lobes are engaged in episodic memory,7 and the lateral parietal cortex is involved in spatial attention.8 However, the precise functions collectively subserved by the DMN are still largely unknown.

Prior studies have evaluated a variety of resting-state networks in adults with mesial temporal lobe epilepsy9–13 and generalized tonic clonic seizures.14–16 Gotman et al9 found that spike and wave discharges in epilepsy were associated with deactivations in the default state of the brain. This deactivation of the resting-state network by epileptiform discharges may be associated with impaired cognitive function in patients with epilepsy. Zhang et al12...
We hypothesized that ictal and/or interictal activity in children with medically refractory epilepsy leads to reduced functional connectivity within the DMN. The secondary hypothesis is that there is an association between impaired DMN and longer duration of epilepsy and impaired IQ. The aim of this study was to determine whether there is a difference in the DMN as measured by using resting-state fMRI in children with poorly controlled epilepsy relative to controls. The secondary aim was to determine whether there is an association between impaired DMN and clinical measures of seizure severity and IQ.

MATERIALS AND METHODS

Subjects

The study was approved by the local institutional research ethics board. Eleven children, mean age of 14.1 ± 2.1 years (range, 10.0–16.3 years), consisting of 6 girls and 5 boys with medically refractory epilepsy who were being evaluated for epilepsy surgery were recruited (Table 1). The mean age of seizure onset was 8.6 ± 3.4 years, the mean duration of epilepsy was 5.4 ± 3.8 years, and the mean seizure frequency was 14.4 per week (range, 2–40). The mean number of medications in patients was 1.9 (range, 1–3). Seven patients had complex partial seizures, 1 had complex partial seizures with secondary generalization, 2 had simple partial seizures, and 1 had simple partial seizures with secondary generalization. Video EEG and seizure semiology localized the seizure to the frontal lobe in 6 patients (including 3 in the paracentral region), the neocortical temporal lobe in 3 patients, the right lateral parietal-occipital lobe in 1 patient, and the right hemisphere in 1 patient. All the children with epilepsy had normal MR imaging findings and no neurologic or psychiatric disorders were included. The mean age of the controls was 14.5 ± 2.4 years (range, 10.7–16.9 years). There was no significant difference between the ages of the patients and controls (P > .05).

MR Imaging

MR imaging was performed on a 3T scanner (Achieva magnet; Philips Healthcare, Best, the Netherlands) by using an 8-channel phased array head coil in all patients and controls. Patients were imaged by using the epilepsy protocol, which included axial and coronal FLAIR (TR/TE = 10,000/140 ms, section thickness = 3 mm, FOV = 22 cm, matrix = 316 × 290), axial and coronal T2 and proton attenuation (TR/TE = 4200/80/40 ms, section thickness = 3 mm, FOV = 22 cm, matrix = 400 × 272), volumetric 3D T1 (TR/TE = 4.9/2.3 ms, section thickness = 1 mm, FOV = 22 cm, matrix = 220 × 220), and resting-state fMRI (TR = 2000 ms, TE = 30 ms, flip angle = 90°, FOV = 220 cm, matrix = 88 × 86 mm, section thickness = 5 mm, 180 volumes acquired and aligned to the anterior/posterior commissure line). Resting-state fMRI was performed with the patient’s eyes closed. The imaging in controls included axial FLAIR, T2 and proton attenuation, volumetric 3D T1, and resting-state fMRI, which were performed with the same parameters as those in patients. The 3T MRI of patients and controls were reviewed by a pediatric neuroradiologist (E.W.) with expertise in epilepsy imaging, to verify that there was no lesion seen on MR imaging.

Data Preprocessing

A series of data-preprocessing steps were carried out by using both AFNI (http://afni.nimh.nih.gov/) and FSL (http://www.fmrib.ox.ac.uk/fsl/) software packages. The details of the pre-processing steps are as follows: To allow T1 equilibrium effects, we discarded the first 10 volumes of each fMRI run. All volumes of the fMRI dataset were rigidly registered to the first volume of the same run (3dvolreg; AFNI). Section-timing correction was then performed on the motion-corrected data (3dTshift; AFNI). The differences in translational and rotational head motion between the patient and control groups were assessed.20 There were no significant differences for translational motion (P = .4995) and rotational motion (P = .2271) between the 2 groups. Next, both the anatomic T1 and the fMRI datasets were skull-stripped by using AFNI. To achieve atlas registration, we aligned the fMRI image to the high-resolution anatomic T1 image by computing an

Table 1: Clinical characteristics of patients

<table>
<thead>
<tr>
<th>No./Age (yr)/Sex</th>
<th>Location of Epilepsy</th>
<th>Age at Seizure Onset (yr)</th>
<th>Duration of Epilepsy (yr)</th>
<th>Antiepileptic Medications</th>
<th>Seizure Frequency/Week</th>
</tr>
</thead>
<tbody>
<tr>
<td>1/15.2/F</td>
<td>R Frontal</td>
<td>7</td>
<td>8</td>
<td>Lamotrigine, levetiracetam</td>
<td>7</td>
</tr>
<tr>
<td>2/16.3/F</td>
<td>R Frontal paracentral</td>
<td>14</td>
<td>2.3</td>
<td>Carbamazepine</td>
<td>7</td>
</tr>
<tr>
<td>3/10.0/F</td>
<td>R neocortical inferior temporal</td>
<td>7</td>
<td>3</td>
<td>Lamotrigine, topiramate</td>
<td>10</td>
</tr>
<tr>
<td>4/15.3/F</td>
<td>R Frontal paracentral</td>
<td>3</td>
<td>12.3</td>
<td>Carbamazepine, lamotrigine, divalproex</td>
<td>10</td>
</tr>
<tr>
<td>5/14.0/M</td>
<td>L Frontal</td>
<td>8</td>
<td>6</td>
<td>Valproic acid, lamotrigine</td>
<td>20</td>
</tr>
<tr>
<td>6/10.1/F</td>
<td>L neocortical anterior temporal</td>
<td>8</td>
<td>2</td>
<td>Carbamazepine</td>
<td>10</td>
</tr>
<tr>
<td>7/16.2/M</td>
<td>L Frontal paracentral</td>
<td>8</td>
<td>8</td>
<td>Carbamazepine, levetiracetam</td>
<td>10</td>
</tr>
<tr>
<td>8/14.1/M</td>
<td>L neocortical anterior temporal</td>
<td>12</td>
<td>2</td>
<td>Lamotrigine, levetiracetam</td>
<td>2</td>
</tr>
<tr>
<td>9/14.7/F</td>
<td>R hemisphere</td>
<td>13</td>
<td>1</td>
<td>Levetiracetam, divalproex, valproic acid</td>
<td>2.5</td>
</tr>
<tr>
<td>10/15.0/F</td>
<td>L Frontal</td>
<td>4.5</td>
<td>10.5</td>
<td>Oxcarbazepine</td>
<td>40</td>
</tr>
<tr>
<td>11/14.1/F</td>
<td>R lateral parietal occipital</td>
<td>10</td>
<td>4</td>
<td>Levetiracetam, topiramate</td>
<td>40</td>
</tr>
</tbody>
</table>

Note: —R indicates right; L, left.
affine transformation (Linear Image Registration Tool of fMRI of the Brain; FSL). The T1 image was then affine-registered to MNI152 brain template of the Montreal Neurological Institute. The 3 transformations were then concatenated and used to resample the fMRI image to the MNI atlas space with a 2-mm isotropic voxel resolution. The fMRI data were then spatially smoothed by using a Gaussian kernel of 8-mm full width at half maximum.

Independent Component Analysis
To identify the DMN, we used spatial IC analysis to decompose the data of all individuals in both groups into 25 ICs. IC analysis aims to identify temporally coherent networks by estimating maximally independent spatial sources. Each component is associated with a waveform that corresponds to the temporal profile of a specific pattern of coherent brain activity and a spatial map that expresses the intensity with which this connectivity is found across the voxels. We used the Infomax algorithm implemented in the group IC analysis of the fMRI Toolbox (GIFT) (http://mialab.mrn.org/software/gift/, Version 2.0e). The number of components for each individual subject was estimated by using the minimum description length criterion built into GIFT. The average of individual IC numbers (ie, 25) was then used for all the individuals.

All ICs were spatially correlated with a DMN template (within the GIFT toolbox). The DMN template included the bilateral lateral parietal cortex, the mPFC, PCC/PCUN, and medial temporal lobes. The component corresponding to the DMN was then extracted from all subjects in both groups. Intensity values in each spatial DMN map were converted to z scores to reflect the degree to which the time-series of each voxel correlates with the time-series of the DMN component, scaled by the SD of the error term. In other words, the z score is a measure of how many SDs the signal is from the background noise.

Within- and Between-Group Analysis of the DMN
A random-effects analysis was performed on the Z-maps of the DMN within each group by using a 1-sample t test. Thresholds were set at \( P < .05 \), after correction for multiple comparisons by using the false discovery rate. Next, a 2-sample t test was performed to compare the Z-maps of the DMN between the patient and control groups. In this case, the threshold was set at \( P < .05 \), and a minimum cluster size of 15 voxels was used. The group comparison was masked to the voxels within the networks of either the control or patient groups (as defined by t test, \( P < .05 \), false discovery rate–corrected).

Functional Connectivity within the DMN
Four ROIs in the PCC/PCUN, mPFC, and left/right lateral parietal cortices were selected from the false discovery rate–corrected DMN map of the control group. The same ROIs were used in both the patient and control groups. The following preprocessing steps were performed on each region of interest: First, the average time-series was extracted from each region of interest. Then, linear regression analysis was used to remove several sources of spurious variance, which were unlikely to represent regionally specific correlations of neuronal origin. The nuisance variables included the 6 parameters obtained from rigid-body head-motion correction, and the signal was averaged over the time-series of 3 CSF and 6 white matter ROIs located in different regions of the brain. All these signals were regressed out simultaneously by using the 3dDeconvolve program in AFNI. The residual average time-series after regression was used for further pair-wise correlation analyses. To quantify the functional connectivity within the DMN, we used the Pearson correlation to calculate temporal correlation coefficients between all 6 pairs of ROIs.

Correlation between Connectivity in the DMN and Clinical Parameters
The relations between z scores of the temporal correlation coefficients between 6 pairs of ROIs and clinical seizure parameters, including age at seizure onset, duration of epilepsy, number of med-
ications, seizure frequency, and IQ, were assessed by using the Pearson correlation.

RESULTS
Functional Connectivity of the DMN in Each Group
The random-effects analyses of IC maps in the patient and control groups showed the spatial pattern of the DMN (P < .05 after false discovery rate) (Fig 1). The DMN pattern in the controls demonstrated functional connectivity among the PCC/PCUN, mPFC, and bilateral lateral parietal cortex (Fig 1A and Table 2). The DMN pattern of the patients showed similar regions of functional connectivity, as shown in Fig 1B. The patients demonstrated decreased DMN connectivity in the PCC/PCUN, bilateral lateral parietal cortex, and anterior and midcingulate (Fig 1C and Table 3).

Functional Connectivity of the DMN between Patients and Controls
The z scores of the 6 pairs of functional connectivity in patients and controls are shown in Fig 2. There was reduced connectivity between the following pairs of ROIs in patients compared with controls: the mPFC–right lateral parietal cortex (P = .0252), the PCC/PCUN–left lateral parietal cortex (P = .008), and the PCC/PCUN–right lateral parietal cortex (P = .0101). There were no significant differences between the following pairs of ROIs in patients relative to controls: right lateral parietal cortex–left lateral parietal cortex (P = .0756), mPFC–left lateral parietal cortex (P = .0931), and PCC/PCUN–mPFC (P = .0984). None of the pairs of regions of interest demonstrated increased connectivity in patients relative to controls.

Correlation between Connectivity in the DMN and Clinical Parameters
There were no significant correlations between the z scores of the temporal correlation coefficients of the 6 pairs of ROIs in patients and age of seizure onset (P > .05 for all), duration of epilepsy (P > .05), number of medications (P > .05), and seizure frequency (P > .05). IQ was lower in patients (mean, 98.5 ± 14.8) than in controls (mean, 110.0 ± 9.8) (P = .043). No significant correlations were detected between the z scores of the temporal coefficient of the 6 pairs of ROIs in patients and IQ (P > .05 for all).

DISCUSSION
Using resting-state fMRI, we have found impaired connectivity within the DMN in children with poorly controlled epilepsy, with reduced connectivity between the mPFC–right lateral parietal cortex, PCC/PCUN–left lateral parietal cortex, and the PCC/PCUN–right lateral parietal cortex. This reduction in functional connectivity may be related to a variety of factors, including ictal

Table 2: Location of brain regions in the default mode network of the controls

<table>
<thead>
<tr>
<th>Anatomic Regions</th>
<th>Hemisphere</th>
<th>MNI Coordinates (x, y, z)</th>
<th>Peak T Value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Posterior cingulate cortex/precuneus</td>
<td>L/R</td>
<td>-6, -54, 28</td>
<td>15.87</td>
</tr>
<tr>
<td>Medial prefrontal cortex</td>
<td>L/R</td>
<td>-4, 58, -10</td>
<td>13.89</td>
</tr>
<tr>
<td>Lateral parietal cortex</td>
<td>L</td>
<td>-44, -62, 33</td>
<td>9.91</td>
</tr>
<tr>
<td></td>
<td>R</td>
<td>42, -63, 33</td>
<td>10.51</td>
</tr>
</tbody>
</table>

Note: —R indicates right; L, left.

*P < .05 after correction for multiple comparison using false discovery rate.

Table 3: Regions demonstrating reduced connectivity in patients relative to controls

<table>
<thead>
<tr>
<th>Anatomic Regions</th>
<th>MNI Coordinates (x, y, and z)</th>
<th>Voxel Size (mm³)</th>
<th>Peak T Value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Right anterior cingulate</td>
<td>4.40, 8</td>
<td>75</td>
<td>3.549</td>
</tr>
<tr>
<td>Right midcingulate</td>
<td>4, -16, 40</td>
<td>55</td>
<td>2.679</td>
</tr>
<tr>
<td>Right posterior cingulate cortex/precuneus</td>
<td>10, -68, 52</td>
<td>23</td>
<td>2.214</td>
</tr>
<tr>
<td>Right lateral parietal cortex</td>
<td>42, -52, 56</td>
<td>183</td>
<td>3.606</td>
</tr>
<tr>
<td>Left lateral parietal cortex</td>
<td>-36, -62, 56</td>
<td>142</td>
<td>4.187</td>
</tr>
<tr>
<td>Left posterior cingulate cortex/precuneus</td>
<td>0, -60, 34</td>
<td>91</td>
<td>2.682</td>
</tr>
</tbody>
</table>

FIG 2. Functional connectivity within the DMN in controls (A) and patients (B). Numbers in the rectangles correspond to the average pair-wise correlation coefficients. C. Comparison of functional connectivity within the DMN in controls versus patients shows significant reduction in mPFC–right lateral parietal cortex (LPC), PCC/PCUN–right LPC, and PCC/PCUN–left LPC. Numbers in rectangles represent the P value for the comparison of the mean correlation coefficients of control and patient groups. Thick lines represent significant changes in the pair-wise correlation between controls and patients (P < .05).
and interictal epileptiform discharges, frequent spread of seizure activities, and malformations of cortical development, that are not apparent on MR imaging. We have used IC analysis to retrieve patterns of coherent functional connectivity across all voxels in the brain, which permits evaluation of global connectivity. IC analysis has the advantage of not having to specify a priori the anatomic ROIs of the network.

Previous studies have reported a reduction in functional connectivity in the resting-state networks or a combination of reduced and increased connectivity in the resting-state networks in adults with epilepsy. Wang et al previously evaluated the resting-state networks in patients with generalized tonic clonic seizures and have found regions of decreased as well as increased functional connectivity in the DMN and dorsal attention networks. Bettus et al evaluated the basal functional connectivity in adults with medial temporal lobe epilepsy and found that in those with left medial temporal lobe epilepsy, there was a trend toward decreased connectivity of the left anterior and posterior hippocampi link and a trend toward increased connectivity of the right anterior and posterior hippocampi link. Mankinen et al evaluated the resting-state connectivity of children with non-sional temporal lobe epilepsy. They found reduced connectivity in the anterior component of the DMN, visual dorsal cortex, and pontine and somatosensory cortex resting-state network.

Subgroup analysis of patients with temporal lobe epilepsy and abnormal EEG findings showed reduced connectivity in 4 ICs and increased connectivity in 1 component, while those with temporal lobe epilepsy and normal EEG findings had reduced connectivity in 3 ICs. The reduction in functional connectivity is thought to reflect a dysfunction in the network, while an increase in functional connectivity is thought to reflect a compensatory mechanism or reorganization of the network. We did not find an increase in the functional connectivity in the DMN, a result similar to that reported in the study by Liao et al. It is possible that some seizure types or functional networks or certain epileptogenic substrates such as hippocampal sclerosis may be more likely associated with compensatory increased connectivity than others or that there is a period of time with epilepsy that is necessary before the compensation is observed. Further work is needed to clarify which patient populations, functional networks, or epileptogenic substrates are more likely to be associated with compensatory increased connectivity and to determine the clinical relevance of this compensatory connectivity.

We have not found a correlation between the strength of connectivity in the DMN and clinical parameters such as age at seizure onset, duration of epilepsy, number of medications, and seizure frequency. Wang et al found a negative correlation between seizure duration and functional connectivity in the medial prefrontal cortex in patients with generalized tonic clonic seizures. Zhang et al also found a negative correlation between epilepsy duration and the mean z values within the regions that showed reduced functional connectivity in the visual, auditory, and sensorimotor networks in patients with temporal lobe epilepsy. The difference in the findings between the reported studies and our findings could be related to differences in the duration of epilepsy. The mean duration of epilepsy in those studies in adults varied from 10.6 to 13.0 years, which was at least twice as long as the mean duration of epilepsy in our patients. Longer duration of epilepsy may lead to greater impairment in resting-state networks. Alternatively, the more homogeneous group of patients with a specific type of epilepsy in those studies may have contributed to the observed association between epilepsy duration and resting-state functional connectivity. The lack of correlation between the strength of the connectivity in the DMN and clinical parameters in our study could also be related to the relatively small sample size and variations in seizure types. We did not identify an association between the number of antiepileptic medications and impaired DMN. However, this does not preclude the possibility of specific antiepileptic medications exerting a negative influence on resting-state connectivity.

We have not identified the medial temporal lobe component of the DMN within the patient and control groups. Because the medial temporal lobe is located close to the skull base and sphenoid sinus, it is possible that gradient artifacts reduce the signal from the medial temporal lobe. Failure to identify the medial temporal lobe is unlikely due to immaturity of the DMN in children. Supelka et al found that the DMN, including the medial temporal lobe component, could be identified in children 7–9 years of age and that the connectivity and strength of the medial temporal lobe was similar in children and adults. One of the potential limitations of this study is the small number of patients with a wide variety of partial seizures. Despite the variations in seizure types, we found reduced connectivity in the DMN. Impairment in the DMN does not appear to be specific to the subtypes of seizures and has been described in temporal lobe epilepsy, generalized tonic clonic seizures, and absence of epilepsy. Certain types of epilepsy, such as mesial temporal lobe epilepsy, could have a direct influence on the DMN because the seizure focus included the medial temporal lobe component of the DMN.

In our study, in some patients such as case 11, the seizure focus in the right lateral parietal occipital lobe included the lateral parietal cortex component of the DMN, but in others, such as those with seizures arising from the neocortical temporal lobe (cases 3, 6, and 8) or paracentral region (cases 2, 4, and 7), the seizure focus did not include the DMN. Hence, other factors, such as frequent spread of seizure activities, may have contributed to the reduced connectivity in the DMN, in addition to the epileptiform discharges within the seizure focus. It is not known whether patients with generalized epilepsy are more likely to have greater impairment in some resting-state networks such as the DMN relative to patients with partial epilepsy and whether those with partial epilepsy and secondary generalization are more likely to have greater impairment in resting-state networks than those with partial epilepsy but without secondary generalization. Due to the small number of patients with partial epilepsy and secondary generalization, we have not performed subgroup analysis. Another limitation of this study was that we have not assessed those cognitive functions subserved by the DMN, such as autobiographic memory, episodic memory, and social cognitive function. We have assessed the IQs of patients and controls and have found no correlation between impaired IQ and reduced functional connectivity. Although IQ provides a global measure of cognitive function, it is not directly related to DMN.
CONCLUSIONS

We have found reduced connectivity in the DMN in children with medically refractory epilepsy. Further study is needed to determine whether different types of seizures have different effects on the strength of connectivity within the DMN. In addition, simultaneous recording of EEG during the DMN determination would allow us to determine whether interictal spikes and spike-wave activity on the EEG correlate with alteration of the DMN. We have not found an association between reduced connectivity in the DMN and reduced IQ. However, correlation study between DMN and cognitive functions subserved by the network, such as autobiographic memory, episodic memory, and attention, is needed to further understand the significance of the impaired connectivity in the DMN.

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