Dynamic Contrast-Enhanced Perfusion MR Imaging Measurements of Endothelial Permeability: Differentiation between Atypical and Typical Meningiomas

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AJNR Am J Neuroradiol 2003, 24 (8) 1554-1559
http://www.ajnr.org/content/24/8/1554
Dynamic Contrast-Enhanced Perfusion MR Imaging Measurements of Endothelial Permeability: Differentiation between Atypical and Typical Meningiomas

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BACKGROUND AND PURPOSE: The measurement of relative cerebral blood volume (rCBV) and the volume transfer constant ($K^{\text{trans}}$) by means of dynamic contrast-enhanced (DCE) perfusion MR imaging (pMRI) can be useful in characterizing brain tumors. The purpose of our study was to evaluate the utility of these measurements in differentiating typical meningiomas and atypical meningiomas.

METHODS: Fifteen patients with pathologically confirmed typical meningiomas and seven with atypical meningiomas underwent conventional imaging and DCE pMRI before resection. rCBV measurements were calculated by using standard intravascular indicator dilution algorithms. $K^{\text{trans}}$ was calculated from the same DCE pMRI data by using a new pharmacokinetic modeling (PM) algorithm. Results were compared with pathologic findings.

RESULTS: Mean rCBV was 8.02 ± 4.74 in the 15 typical meningiomas and 10.50 ± 2.1 in the seven atypical meningiomas. $K^{\text{trans}}$ was 0.0016 seconds$^{-1}$ ± 0.0012 in the typical group and 0.0066 seconds$^{-1}$ ± 0.0026 in the atypical group. The difference in $K^{\text{trans}}$ was statistically significant ($P < .01$, Student $t$ test). Other parameters generated with the PM algorithm (plasma volume, volume of the extravascular extracellular space, and flux rate constant) were not significantly different between the two tumor types.

CONCLUSION: DCE pMRI may have a role in the prospective characterization of meningiomas. Specifically, the measurement of $K^{\text{trans}}$ is of use in distinguishing atypical meningiomas from typical meningiomas.

Although meningiomas have readily identifiable imaging features, conventional imaging techniques have not always been reliable in predicting the grade or natural history of tumors (1–4). Studies have shown no statistically significant correlation between histologic features and signal intensity on proton density– or T2-weighted images (5). Sometimes, the aggressiveness of the tumor cannot be accurately characterized, even on the basis of histopathologic findings, partly because of sampling error (6, 7).

The World Health Organization (WHO) defines the atypical variant as a meningioma having increased mitotic activity in comparison to the typical meningioma. Other features that can also qualify the lesion as being atypical are increased cellularity and foci of spontaneous or geographic necrosis. More recently, the presence of brain invasion has been described as an important factor in the risk of recurrence (8, 9). The distinction between atypical meningiomas and typical meningiomas is clinically relevant, because benign meningiomas recur in about 7–20% of cases, whereas atypical variants recur in 29–41% (4, 9–11). Furthermore, the aggressiveness of surgical resection and adjunctive radiation therapy is also partly determined by this distinction.

Measurements of the cerebral blood volume (CBV) from dynamic contrast-enhanced (DCE) perfusion MR imaging (pMRI) data have previously been shown to be useful in differentiating gliomas of different grades (12, 13). However, these measurements are based on intravascular indicator dilution
theory (14), which assumes that contrast agent remains intravascular. Because meningiomas lack a true blood-brain barrier, this assumption is violated, and although corrections can be applied, we have noticed that CBV measurements in meningiomas are probably artificially elevated. Therefore, we investigated whether measurements made by using a novel pharmacokinetic modeling (PM) algorithm (15) can help in differentiating typical meningiomas and atypical meningiomas. We hypothesized that atypical meningiomas are associated with a permeability higher than that of typical variants, as expressed by the volume transfer constant \(K_{\text{trans}}\).

**Methods**

We retrospectively analyzed data collected from patients imaged at our institution from March 1996 to January 2003. This retrospective review of cases was approved by our institutional review board.

Data from 22 patients (four male, 18 female; age range, 27–79 years) were evaluated. In all patients, a histopathologic diagnosis was obtained after near-total or total volumetric resection by two experienced neuropathologists (D.Z., H.H.W.). In 15 patients, meningioma, typical variant (WHO grade I/III), was diagnosed. In seven patients, atypical meningioma (WHO grade II/III) was diagnosed.

Imaging was performed on 1.5-T machines (Siemens AG; Siemens, Erlangen, Germany). Images were acquired by using our standard protocol for the assessment of intracranial lesions. A localizing sagittal T1-weighted image was obtained, followed by nonenhanced axial T1-weighted (TR/TE, 600/14), intermediate-weighted (3400/17), and T2-weighted (3400/119) images. A series of 60 gradient-echo echo-planar images (1000/54) were acquired at 1-second intervals during the first pass of a standard bolus (0.1 mmol/kg) gadopentetate dimeglumine (Magnevist; Berlex, Wayne, NY). The contrast agent was injected at a rate of 5 mL/s, followed by a bolus of sodium chloride solution injected at a rate of 5 mL/s after the 10th baseline acquisition. Six or seven 5-mm-thick sections were acquired. These were positioned from the T2-weighted images to cover the entire tumor.

**Image Processing**

Data processing was performed offline by using a postprocessing workstation (Sparestation; Sun Microsystems, Palo Alto, CA) with programs developed inhouse by using the C and IDL programming languages (RSI, Boulder, CO).

**Intravascular Indicator Dilution Theory**

Relative CBV (rCBV) values were calculated by using standard algorithms based on the intravascular indicator dilution theory (14). The methods for acquiring perfusion data from a set of DCE echo-planar images have been fully described previously (13).

CBVs were measured in regions of interest (ROIs) positioned within the tumor and expressed relative to measurements made in an ROI in the contralateral white matter. ROIs were positioned in areas of maximal abnormality on the basis of color maps. To minimize confounding factors in the rCBV analysis, the size of the ROIs was kept constant (radius, 3.6 mm). Also, measurement of the maximal abnormality, at least in rCBV measurements, has been demonstrated to provide the highest intraobserver and interobserver reproducibility (16).

First-Pass PM

A new algorithm (15) that allows the simultaneous calculation of blood plasma volume \(v_p\) and \(K_{\text{trans}}\) was also applied to the dynamic data. The algorithm, first-pass PM, used an exact expression for the concentration of contrast material in the tissue, assuming that contrast exists in the two exchanging compartments (plasma and extravascular extracellular space [EES]). An estimate of the vascular contrast-agent concentration was acquired from normal white matter and fitted to the expression for the tissue concentration to derive \(v_p\), \(K_{\text{trans}}\), and the volume of the EES \(v_e\). The flux rate constant \(k_{\text{ep}} = K_{\text{trans}}/v_p\) was also calculated from the measured \(K_{\text{trans}}\) and \(v_p\). \(K_{\text{trans}}\), \(v_p\), and \(v_e\) were measured in the same ROIs in which the rCBV was measured.

**Statistical Analysis**

The Student \(t\) test was used to determine whether calculated hemodynamic parameters were significantly different in typical meningiomas and atypical meningiomas. A \(P\) value of less than .05 was considered to indicate a statistically significant difference, and no correction for multiple comparisons was made.

**Results**

The Table summarizes the hemodynamic parameters from the series studied. rCBV values ranged from 1.99 to 17.8 in the typical group \((n = 15)\), with a mean of 8.02 \pm 4.74. rCBV values in the atypical group \((n = 7)\) ranged from 8.2 to 13.9, with a mean of 10.50 \pm 2.1. \(K_{\text{trans}}\) was 0.0016 seconds\(^{-1}\) \pm 0.0012 in the typical meningiomas and 0.0066 seconds\(^{-1}\) \pm 0.0026 in the atypical meningiomas. The difference in \(K_{\text{trans}}\) was statistically significant \((P < .01, \text{Student} \ t\ \text{test})\).

A scatterplot depicting rCBV versus \(K_{\text{trans}}\) in grade II atypical meningiomas versus grade I typical meningiomas demonstrated good separation in the permeability measure but not in the rCBV (Fig 1).

In the atypical and typical groups, differences in \(v_p\), \(v_e\), and \(k_{\text{ep}}\) were not statistically significant.

**Discussion**

The grade of a meningioma has important therapeutic and prognostic implications. Thus, prospectively identifying the histologic grade of a meningioma by using DCE pMRI can be clinically beneficial. In most cases, total surgical resection is planned when it is technically feasible. Preoperatively knowing that one is dealing with a high-grade atypical meningioma can lead to alterations in the planned size, shape, and extent of a craniotomy to ensure clean margins. Preoperative knowledge of an atypical meningioma may also change a neurosurgeon’s risk-benefit assessment. In other words, a surgeon may be more aggressive in his or her surgical technique to achieve a complete or Simpson grade I resection (17).

Results of previous studies have shown that the addition of adjuvant radiation therapy improves disease-free survival (18–20). Furthermore, specific parameters regarding the adjuvant dosage have been suggested for the treatment of atypical and malignant grades (21). Therefore, knowing the grade of the
rCBV and \(K^{\text{trans}}\) data in 22 patients with typical or atypical meningiomas

<table>
<thead>
<tr>
<th>Patient/Age, y/Sex</th>
<th>rCBV*</th>
<th>(K^{\text{trans}}, \text{seconds}^{-1})</th>
<th>(v_p, %)</th>
<th>(v_e, %)</th>
<th>(k_{ep}, \text{days}^{-1})</th>
<th>Location</th>
</tr>
</thead>
<tbody>
<tr>
<td>Typical meningiomas</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>1/27/F</td>
<td>9.3</td>
<td>(2.1 \times 10^{-3})</td>
<td>0.87</td>
<td>3.06</td>
<td>(6.9 \times 10^{-4})</td>
<td>Right temporal</td>
</tr>
<tr>
<td>2/33/M</td>
<td>17.8</td>
<td>(2.8 \times 10^{-3})</td>
<td>10.94</td>
<td>0.20</td>
<td>(1.4 \times 10^{-3})</td>
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</tr>
<tr>
<td>3/38/F</td>
<td>14.2</td>
<td>(1.8 \times 10^{-3})</td>
<td>9.9</td>
<td>0.19</td>
<td>(9.1 \times 10^{-3})</td>
<td>Left frontal</td>
</tr>
<tr>
<td>4/41/F</td>
<td>8.7</td>
<td>(1.5 \times 10^{-3})</td>
<td>2.79</td>
<td>8.19</td>
<td>(1.8 \times 10^{-4})</td>
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</tr>
<tr>
<td>5/42/F</td>
<td>4.1</td>
<td>(1.8 \times 10^{-3})</td>
<td>1.23</td>
<td>1.61</td>
<td>(1.2 \times 10^{-3})</td>
<td>Right cerebellopontine</td>
</tr>
<tr>
<td>6/42/F</td>
<td>15.8</td>
<td>(1.9 \times 10^{-3})</td>
<td>12.3</td>
<td>0.80</td>
<td>(2.3 \times 10^{-3})</td>
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</tr>
<tr>
<td>7/47/F</td>
<td>9.7</td>
<td>(9.9 \times 10^{-3})</td>
<td>3.88</td>
<td>(1.9 \times 10^{-4})</td>
<td>(0.47)</td>
<td>Right parasagittal</td>
</tr>
<tr>
<td>8/47/F</td>
<td>5.83</td>
<td>(1.7 \times 10^{-3})</td>
<td>1.63</td>
<td>0.38</td>
<td>(4.5 \times 10^{-3})</td>
<td>Right occipital</td>
</tr>
<tr>
<td>9/50/F</td>
<td>4.19</td>
<td>(3.0 \times 10^{-3})</td>
<td>5.92</td>
<td>5.36</td>
<td>(5.8 \times 10^{-4})</td>
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</tr>
<tr>
<td>10/51/F</td>
<td>6.54</td>
<td>(3.3 \times 10^{-3})</td>
<td>2.63</td>
<td>9.63</td>
<td>(3.4 \times 10^{-4})</td>
<td>Right lateral ventricle</td>
</tr>
<tr>
<td>11/53/F</td>
<td>1.99</td>
<td>(9.3 \times 10^{-5})</td>
<td>8.30</td>
<td>(2.3 \times 10^{-2})</td>
<td>(4.0 \times 10^{-3})</td>
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<td>(2.7 \times 10^{-4})</td>
<td>2.11</td>
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<td>(4.7 \times 10^{-3})</td>
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<td>(3.5 \times 10^{-3})</td>
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<td>7.56</td>
<td>(4.6 \times 10^{-4})</td>
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<td>(2.1 \times 10^{-3})</td>
<td>2.47</td>
<td>8.09</td>
<td>(2.6 \times 10^{-4})</td>
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</tr>
<tr>
<td>15/59/M</td>
<td>5.59</td>
<td>(2.0 \times 10^{-4})</td>
<td>6.78</td>
<td>(3.5 \times 10^{-2})</td>
<td>(5.7 \times 10^{-3})</td>
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</tr>
<tr>
<td>Mean</td>
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<td>4.95</td>
<td>3.01</td>
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<td>3.66</td>
<td>(1.2 \times 10^{-1})</td>
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<td></td>
<td></td>
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<tr>
<td>16/46/F</td>
<td>8.97</td>
<td>(1.1 \times 10^{-2})</td>
<td>1.57</td>
<td>13.7</td>
<td>(8.2 \times 10^{-4})</td>
<td>Right parafalcine</td>
</tr>
<tr>
<td>17/49/F</td>
<td>8.2</td>
<td>(6.3 \times 10^{-3})</td>
<td>3.09</td>
<td>5.17</td>
<td>(1.2 \times 10^{-3})</td>
<td>Left parafalcine</td>
</tr>
<tr>
<td>18/52/F</td>
<td>11.4</td>
<td>(8.2 \times 10^{-3})</td>
<td>9.80</td>
<td>36.5</td>
<td>(2.2 \times 10^{-4})</td>
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</tr>
<tr>
<td>19/58/F</td>
<td>12.07</td>
<td>(7.1 \times 10^{-3})</td>
<td>12.02</td>
<td>32.2</td>
<td>(2.2 \times 10^{-4})</td>
<td>Right parietal</td>
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<td>20/58/F</td>
<td>10.45</td>
<td>(3.2 \times 10^{-3})</td>
<td>12.3</td>
<td>1.44</td>
<td>(2.2 \times 10^{-3})</td>
<td>Left frontal</td>
</tr>
<tr>
<td>21/69/F</td>
<td>8.52</td>
<td>(4.6 \times 10^{-3})</td>
<td>2.78</td>
<td>1.68</td>
<td>(2.7 \times 10^{-3})</td>
<td>Right temporal</td>
</tr>
<tr>
<td>22/79/F</td>
<td>13.9</td>
<td>(5.6 \times 10^{-3})</td>
<td>3.58</td>
<td>11.49</td>
<td>(4.9 \times 10^{-4})</td>
<td>Right frontal</td>
</tr>
<tr>
<td>Mean</td>
<td>10.50</td>
<td>(6.6 \times 10^{-3})</td>
<td>6.45</td>
<td>14.6</td>
<td>(1.1 \times 10^{-3})</td>
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</tr>
<tr>
<td>SD</td>
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<td>(2.59 \times 10^{-3})</td>
<td>4.71</td>
<td>14.3</td>
<td>(9.9 \times 10^{-4})</td>
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</tr>
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</table>

* \(P = .10\).
\(\dagger\) \(P = .002\).
\(\ddagger\) \(P = .48\).
\(\star\) \(P = .08\).
\(\dagger\) \(P = .31\).

Tumor before treatment helps in planning the resection planning and the dose of adjuvant radiation. Histopathologic differentiation is based on the WHO definition, which describes the atypical variant of meningioma as having increased mitotic activity, as well as increased cellularity, foci of spontaneous or geographic necrosis and brain invasion (Fig 2). However, the histopathologic diagnosis may not be as clear cut. On these and other occasions, findings of increased permeability or perfusion can provide the clinician with additional information for determining further neuro-oncologic treatment.

At our institution, the recommendation of the neurosurgeons and neuro-oncologists for the treatment of atypical meningiomas includes follow-up MR imaging every 3 months for the first 12 months, followed

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![Fig 1](https://example.com/fig1.png)

**Fig 1.** Scatterplots of rCBV versus \(K^{\text{trans}}\).

**A.** Grade II (diamonds) versus grade I (squares) meningiomas. The groups are well separated in the permeability measure but not in rCBV.

**B.** rCBV versus \(K^{\text{trans}}\) for the two grades. Data points are the mean values. Error bars indicate the SD.
by yearly MR imaging thereafter. Patients with atypical meningiomas are also considered for external-beam irradiation after resection, regardless of the presence of residual tumor. The dura is thought to be globally abnormal in patients with atypical meningiomas. In patients with recurrent atypical tumors, gamma-knife radiosurgery is sometimes recommended. Previous attempts to prospectively assess the grade of a tumor by using DCE pMRI to measure rCBV were not successful. Notably, Zhu et al (22) found no correlation between rCBV and tumor grade in two malignant and 12 benign meningiomas. In our series of seven atypical and 15 benign meningiomas, this was also the case.

However, a few reports describe the quantitative assessment of vascular permeability in the characterization of meningiomas. Uematsu et al (23), demonstrated the use of T1- and T2*-shortening effects to estimate permeability and vascularity in meningiomas and acoustic neunomas. Although no comparison with atypical meningiomas was made, the investigators found lower permeability in the typical meningioma group than in the neunoma group. This finding is consistent with the results of our comparison of typical and atypical meningiomas (Figs 3 and 4).

The first-pass PM algorithm used in this study has a number of potential advantages over alternative PM algorithms (24). First, most PM algorithms are applied to data during the washout of contrast material when the plasma concentration is low. Taken with the relatively low vascularity of the brain, this approach prevents an accurate assessment of blood (or plasma) volume. The first-pass PM algorithm used data acquired during the first pass when the concentration of contrast material is high. Therefore, as far as we know, first-pass PM is the only algorithm that provides simultaneous estimates of the blood volume, the transfer constant, and the volume of the EES. Second, most PM methods require the acquisition of data over tens of minutes to adequately sample the washout curve. The first-pass PM algorithm requires only first-pass data, which can be acquired in 1 minute or less. Finally, the algorithm uses image data acquired with susceptibility-weighted echo-planar imaging, and

![Fig 2. Photomicrographs (hematoxylin-eosin).](image)

**A**, Medium-power image demonstrates tumor cells, which form a lobulated pattern with whorls (arrows) in a typical meningioma (original magnification ×100).

**B**, High-power images demonstrates at least three mitotic figures (arrows) in this atypical meningioma (original magnification ×200).

![Fig 3. Pathologically confirmed meningioma (WHO grade I/III).](image)

**A**, Axial contrast-enhanced T1-weighted (600/14) MR image.

**B**, Axial gradient-echo (1000/54) pMRI image with an rCBV color overlay demonstrates high rCBV throughout the lesion.

**C**, Axial gradient-echo (1000/54) axial pMRI image with SD25 depicts a decrease in signal intensity after 25 seconds.

**D**, Normalized signal intensity plotted against time for the white matter (squares) and the lesion (triangles). The lines represent the fitted curves derived by using the first-pass PM algorithm. The return to baseline is more rapid in typical meningiomas than in atypical meningiomas.
thus, it can sample as many as about 10 sections with 1-second temporal resolution. Methods such as that of Uematsu et al (23), which involve a combination of T1 and T2* weighting, acquire data more slowly; therefore, they are restricted to single-section acquisitions. T1 effects may have a small impact, even on a first-pass T2*-weighted acquisition. The result is underestimation of the decrease in signal intensity. Currently, we use a 30° flip angle in our protocol to counter this effect.

The finding that $K_{\text{trans}}$ is elevated in atypical meningiomas may reflect their histopathologic characteristics. The relationship of the capillary ultrastructure to the grade of the tumor has not been fully established in meningiomas (25, 26), but the existing literature regarding gliomas suggests that capillary leakiness and the size of endothelial gap junctions are positively correlated with the grade (27–29). One feature often associated with atypical meningiomas, and one possibly related to increased capillary leakiness, is micronecrosis. This micronecrosis is described as spontaneous or geographic necrosis in the WHO model (2). In their study of atypical and malignant meningiomas, McLean et al (3) reported the survival statistics of patients with benign, atypical, or malignant meningiomas. They related the presence of micronecrosis, a feature more prevalent in atypical meningiomas than in typical ones, with the risk of recurrence as well as survival. At 36 months, 32% in patients with micronecrosis survived, and 71% of those without micronecrosis survived. The degree of vascular permeability may possibly be related to the degree of micronecrosis in a meningioma. The lack of correlation between tumor grade and $k_{\text{ep}}$ suggests that the rate of transfer from the intravascular space to the extravascular space is the important element to the equation, rather than the absolute indices of the leakage of contrast material. Naturally, such key parameters are not accessible with conventional imaging, and this limitation may further account for why atypical variants are virtually indistinguishable on conventional contrast-enhanced T1-weighted images.

**Conclusion**

Our data show that an analysis of the dynamic perfusion curves generated by using echo-planar contrast-enhanced T2*-weighted sequences with respect to the permeability between intravascular and extravascular compartments can provide additional information for the preoperative assessment of intracranial meningiomas. This information can be of clinical benefit. We demonstrate good correlation between $K_{\text{trans}}$ and the histologic grade of the meningiomas. Pathologically, the $K_{\text{trans}}$ measurement may be related to the degree of micronecrosis. Because the atypical and typical variants of meningioma have different recurrence rates, $K_{\text{trans}}$ provides one of the few prospective measures of tumor behavior and prognosis. The role of brain invasion in atypical meningiomas, which is known to change the prognosis and treatment, has not been fully explored. The measurement of perfusion parameters in the brain adjacent to meningiomas and their correlation to brain invasion provide an interesting area for future study, and in fact, this project is currently in progress at our institution. Further prospective investigation in a larger cohort of patients with meningiomas is needed, although this work is hindered by the relatively low incidence of atypical or even malignant variants. Intraobserver and interobserver validation studies.
should be performed to demonstrate the reliability and reproducibility of these advanced techniques.

References